

CIMET Thesis 2015

Improvements of the multimodal skin imaging prototype device "SkImager"



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Improvements of the multimodal skin imaging prototype device "SkImager"

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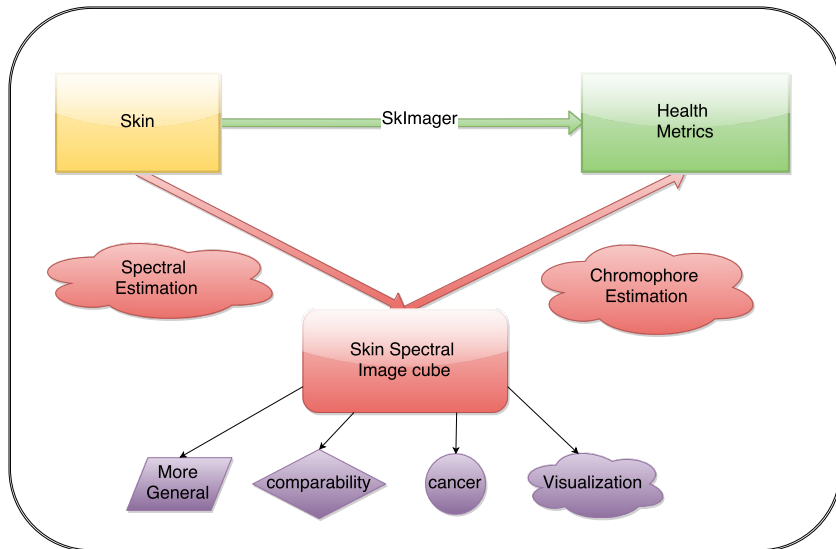
²School of Computing
University of Eastern Finland

16th June 2015

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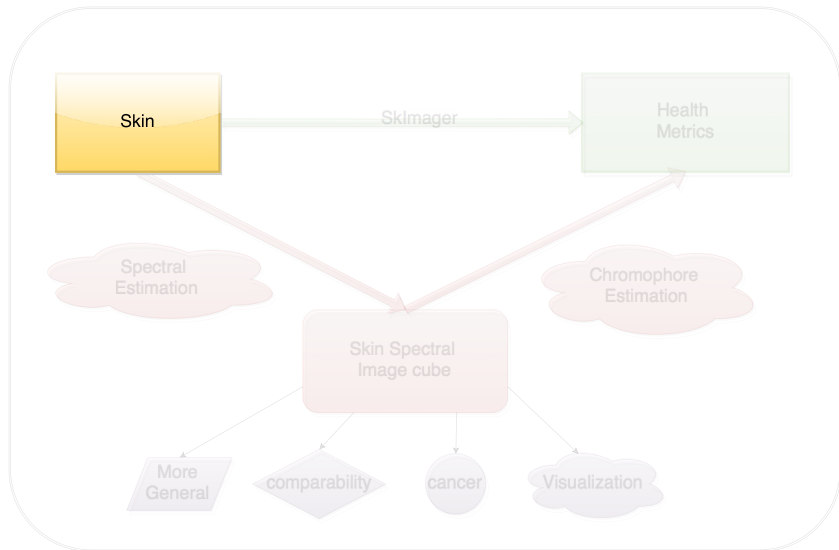
Overview of the Thesis



Explore spectral estimation for a prototype non-contact optical skin assessment device

- Evaluate approaches to use the device
- Investigate computationally efficient methods to obtain more general spectral skin image data
- Demonstrate usefulness of estimations for skin assessment

Background



Spectral Skin Assessment

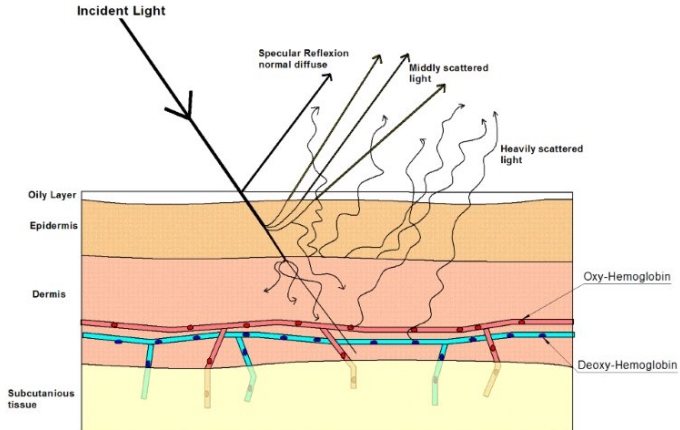


Figure: Simplified skin-light interaction model

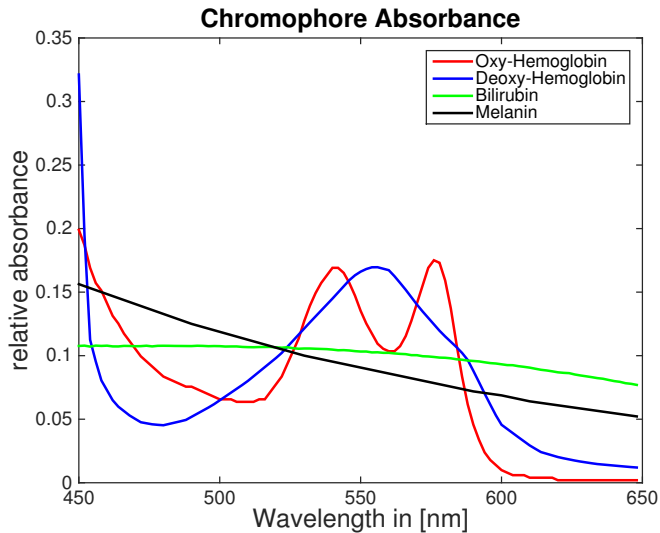
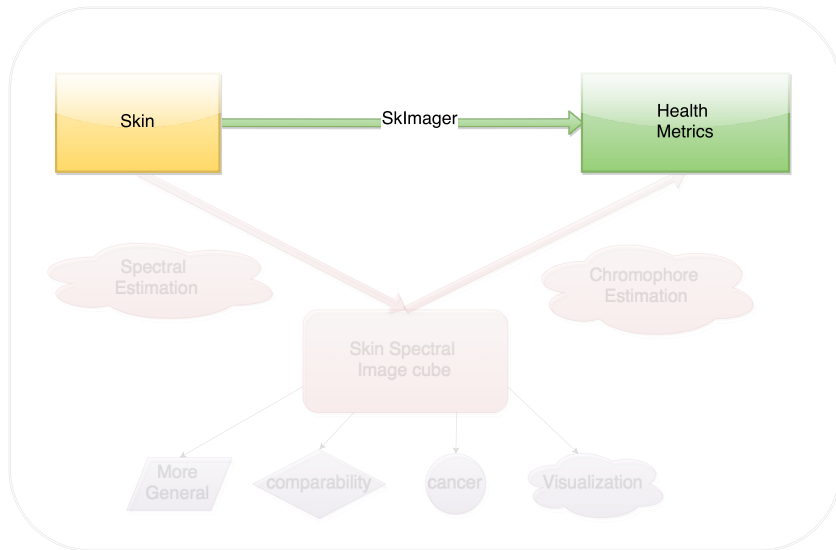
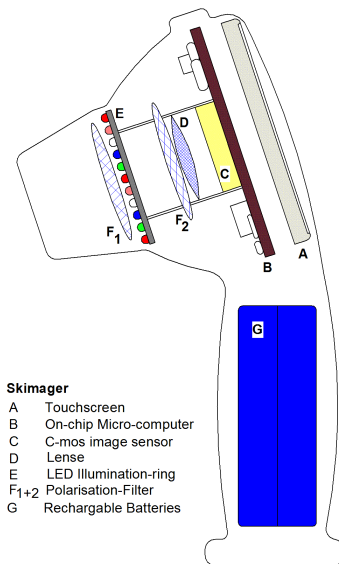


Figure: Common chromophores in skin



The Sklmager



Skimager

- A Touchscreen
- B On-chip Micro-computer
- C C-mos image sensor
- D Lense
- E LED Illumination-ring
- F₁₊₂ Polarisation-Filter
- G Rechargeable Batteries

Sklmager Overview



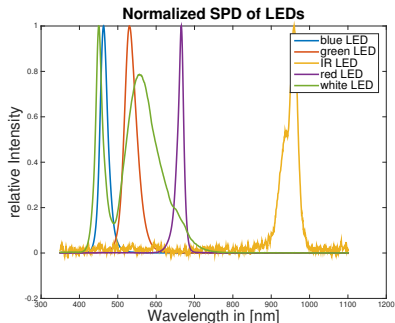
- Sklmager is a proposed non-contact optical skin assessment device¹
- Cheap sensor
- Multi illumination (5LEDs)
- Fast, easy to use,

¹Janis Spigulis et al. "Sklmager: a concept device for in-vivo skin assessment by multimodal imaging". In: *Proceedings of the Estonian Academy of Sciences* 63.3 (2014), pp. 213–220

Linearity of the channels

Spectral properties of the Sklmager

a)



b)

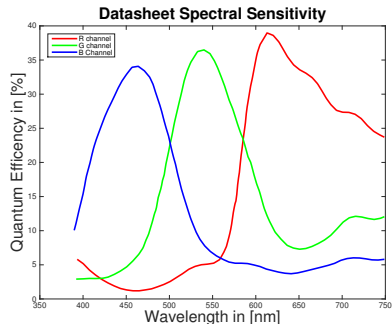


Table: a) Measured normalized LED SPD b) Datasheet sensitivities of the CMOS Sensor³

³ 1/2-Inch 3-Megapixel CMOS Digital Image Sensor. MT9T031. Rev. E 5/11 EN. Aptina. 2006

SNR of the Channels

Red LED	Green LED	Blue LED	White LED	IR LED
SNR: 59.71	SNR: 15.40	SNR: 20.12	SNR: 45.77	SNR: 45.37
SNR: 25.67	SNR: 47.97	SNR: 37.68	SNR: 51.53	SNR: 43.98
SNR: 19.06	SNR: 19.56	SNR: 111.43	SNR: 37.96	SNR: 44.86

Table: All 15 channels of the SkImager with an example image

Current Sklmager Channel approach

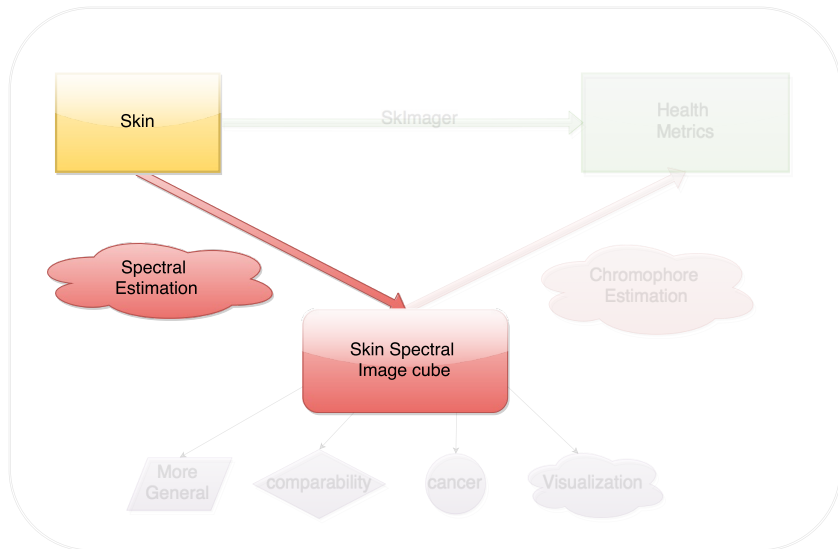
Current Sklmager approach⁴

$$\begin{bmatrix} \Delta OD(R_R) \\ \Delta OD(G_G) \\ \Delta OD(B_B) \end{bmatrix} = \begin{bmatrix} m_1 & m_2 \\ m_3 & m_4 \\ m_5 & m_6 \end{bmatrix} \times \begin{bmatrix} \Delta c_{OH} \\ \Delta c_{DOH} \end{bmatrix}$$

- Only uses 3 channels
- Optical Density is calculated from the channels
- Coefficients m_{1-6} are calculated considering penetration depth and absorbance coefficients for each Chromophore

⁴Dainis Jakovels and Janis Spigulis. "RGB imaging device for mapping and monitoring of hemoglobin distribution in skin". In: *Lithuanian Journal of Physics* 52.1 (2012)

Estimation



Spectral Estimation Overview

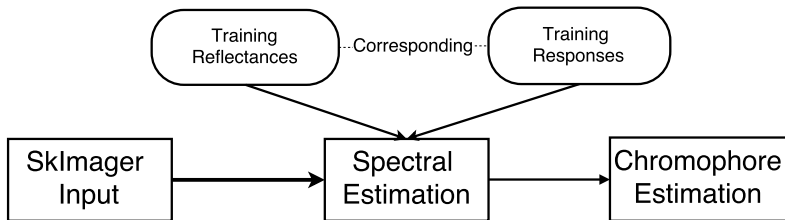
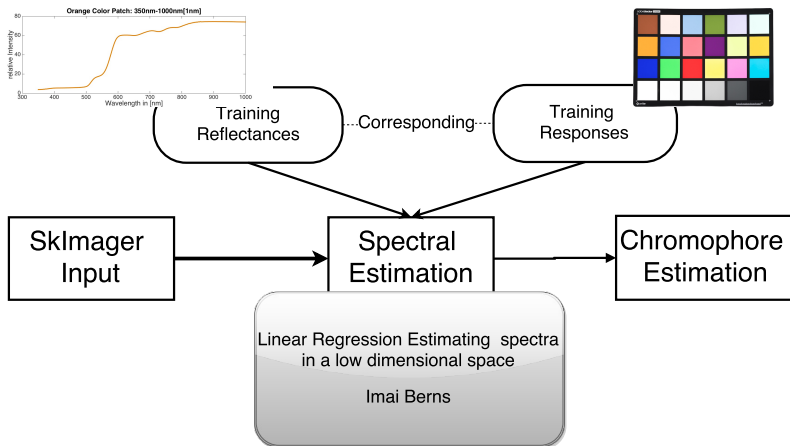


Figure: Overview of the estimation

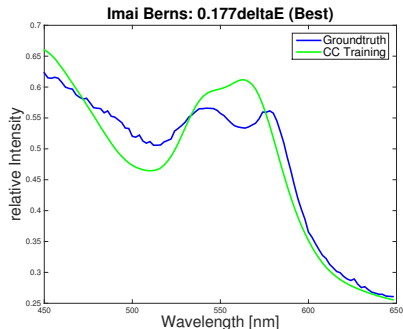
Spectral Estimation Overview



⁴X Rite. X Rite Colorchecker[®]. URL: <http://www.xritephoto.com> (visited on 06/11/2015)

Spectral reconstruction accuracy

a)



b)

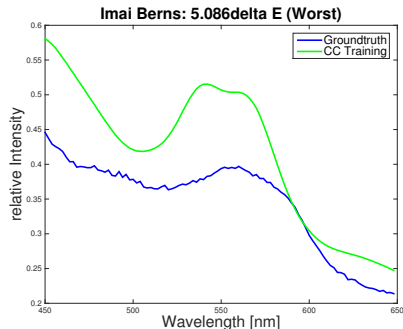


Table: a) Reconstructed spectrum (CC-training) and groundtruth (best ΔE) b) Reconstructed spectrum (CC-training) and groundtruth (worst ΔE)

Spectral reconstruction accuracy

Measure	Min	Max	Avg	Std	95%
RMSE	0.026	0.102	0.044	0.018	0.095
GFC	0.995	0.999	0.997	0.001	0.998
ΔE_{00}	0.177	5.086	1.496	0.917	3.278

Table: Spectral reconstruction tabulated values

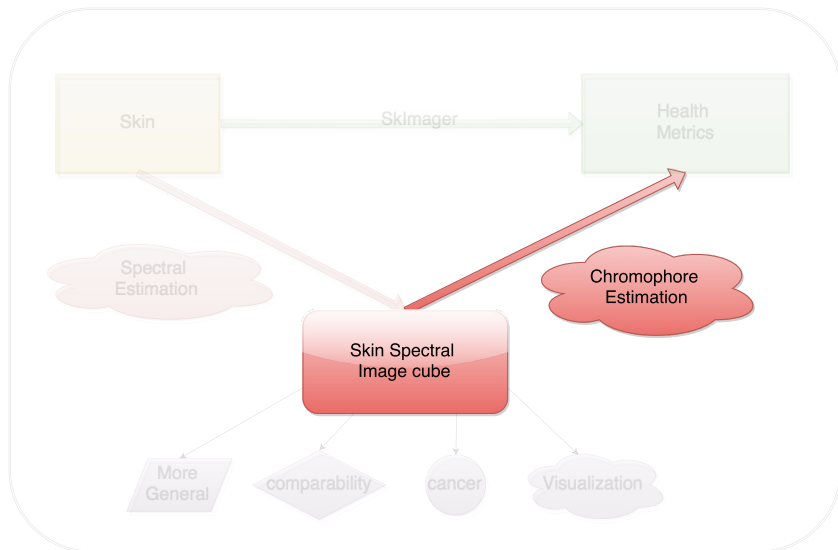
Final Normalization and Conversion

- In order to use the estimated spectra for further processing normalization was performed
- The chromophore estimation requires absorbance curves so the estimated curves are converted using

Conversion to absorbance

$$\tilde{a} = \log_{10}\left(\frac{1}{\tilde{E}_{estimated}}\right)$$

Chromophore Estimation



Chromophore Concentration Estimation

- Chromophore concentration (linear least square fitting) matrix model⁵

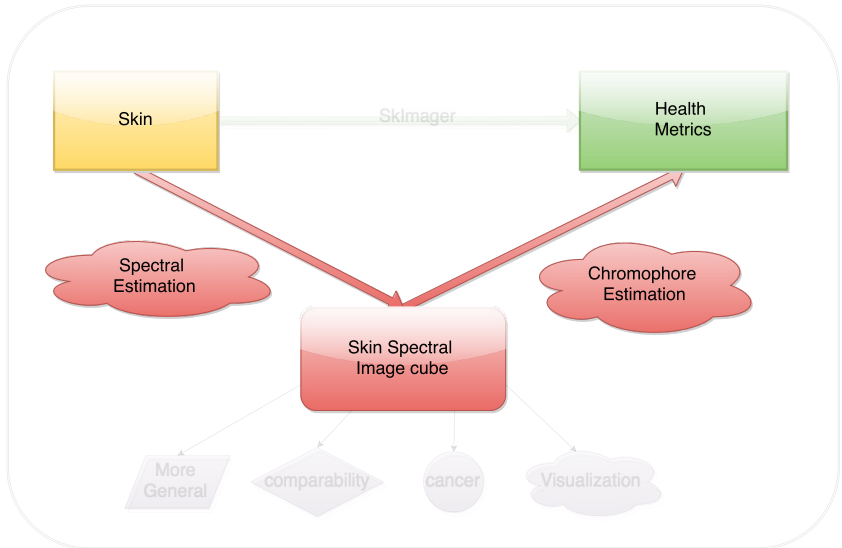
Chromophore concentration estimation

$$C = A * \tilde{E}'$$

- Requires absorbance spectra of chromophores A
- \tilde{E} describes the estimated spectrum per Pixel
- The estimation is performed per pixel (chromophore map)

⁵Petri Välisuo et al. "New closed-form approximation for skin chromophore mapping". In: *Journal of biomedical optics* 16.4 (2011), pp. 046012–046012.

Estimation Results



Test Data

- Two performance evaluations were acquired
- Tests with known test results
- Occlusion measurement for Oxy/Deoxy-Hemoglobin estimation
- Bruise dataset for Bilirubin and Hemoglobin concentration

Occlusion Measurement

- Upper arm occlusion with an inflatable cuff
- 12 patients Caucasian light skinned to medium dark Caucasians (8 men, 4 female)

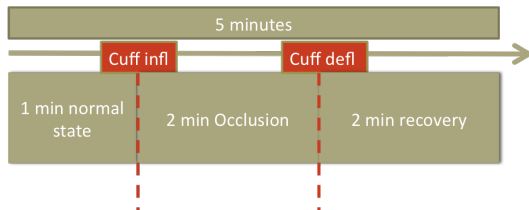
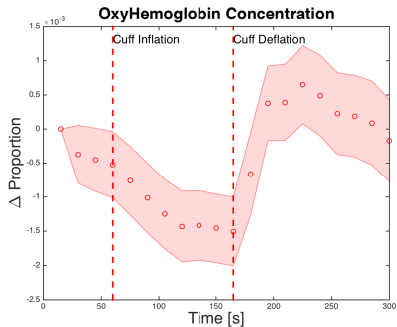


Figure: Temporal overview of the occlusion measurement

- Expected results: exponential decrease of Oxygenated Hemoglobin during occlusion, exponential increase of Deoxygenated Hemoglobin during occlusion

Results

a) Conventional channel approach



b) Estimated spectral workflow

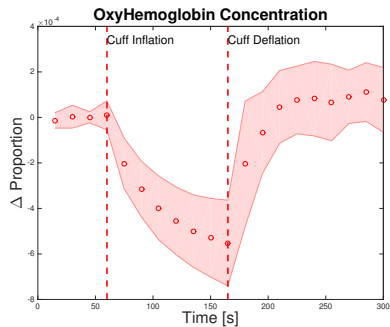
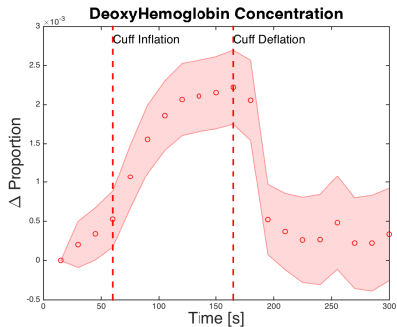


Table: a) Conventional channel approach OxyHemoglobin concentration estimated and averaged over 12 patients and b) Spectrally estimated OxyHemoglobin concentration and averaged over 12 patients using colorchecker training

Results

a) Conventional channel approach



b) Estimated spectral workflow

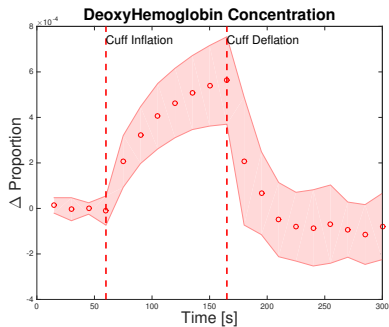


Table: a) Conventional channel approach DeoxyHemoglobin concentration estimated and averaged over 12 patients and b) Spectrally estimated DeoxyHemoglobin concentration and averaged over 12 patients using colorchecker training

Bruise Measurement

- Existing Bruise Dataset
- Patients were bruised using a paintball gun from 2m distance
- Consecutive measurements over 12 days
- Expected outcome: Hemoglobin gets decomposed (concentration decreased), Bilirubin is produced as a byproduct (increasing concentration)

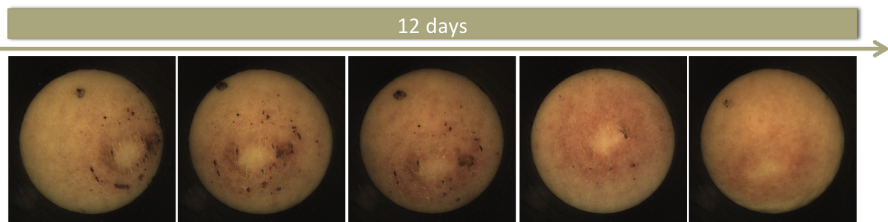
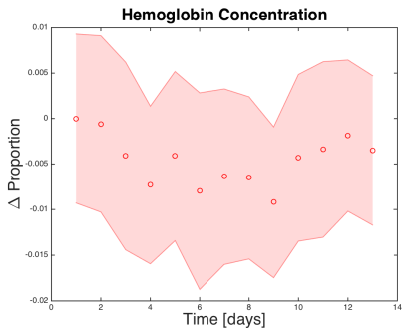


Figure: Bruise dataset example

Results

a)



b)

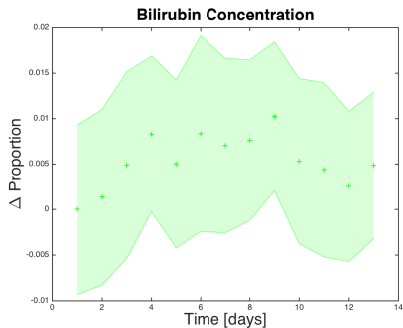
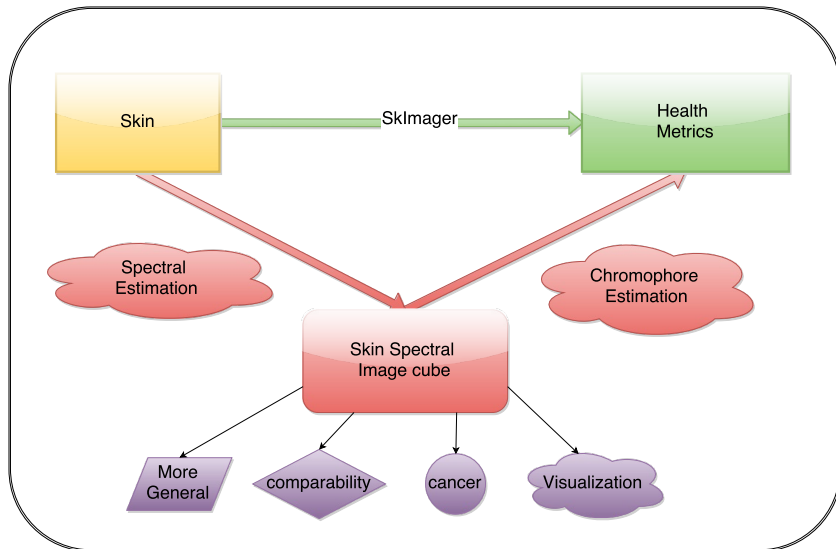


Table: a) Hemoglobin concentration over time b) Bilirubin concentration over time

Conclusions and Furthermore



Conclusion

- Spectral estimation workflow has been established for a low cost handheld skin assessment device
- Good agreement with the current data processing with two well-known experiments has been shown
- More general representation of the data has been acquired for the device

Furthermore







- Spectral estimation can be optimized, more suitable training
- More sophisticated chromophore estimation can be used
- More general estimated spectral data can be used for further analysis i.e. skin lesions, for color corrected visualization, usage of more spectral features

Questions?

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This study has been presented as an oral contribution at the DOC-2015 conference and the NOP-2015 Conference

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