



Remote optical assessment of in-vivo skin: methods, prototype devices and clinical applications

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Towards better skin assessment

- Skin cancer, other diseases → clinicians prefer **compact**, **patient-friendly** and **informative** devices for skin diagnostics;
- Commercial skin imaging devices – still with drawbacks:
 - Low sensitivity/specificity;
 - Insufficient reliability;
 - Bulky design, cable/PC;
 - Able to collect spectral information, but too slowly – motion artifacts create problems; image conversion undeveloped;
 - Expensive, ~20-40 kEUR.



Siascope



DermaLite



MelaFind

Biophotonics Laboratory in Riga

(5...40 co-workers, strongly depending on projects)

Aim – to develop handy and **affordable for end-users** methods, devices and technologies for clinical diagnostics and monitoring by exploiting **optical** features of *in-vivo skin*.

Non-invasive → **non-contact imaging** technologies:

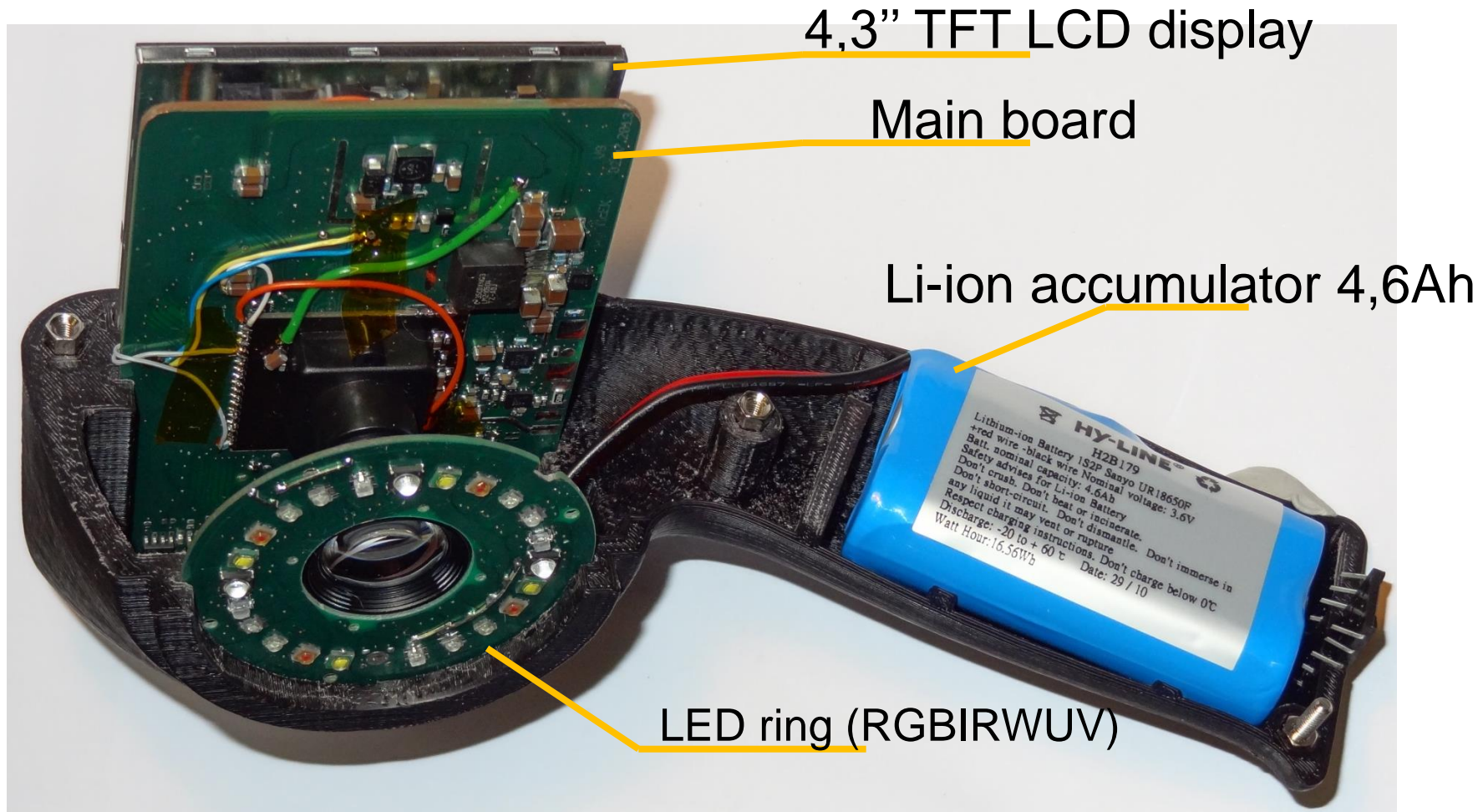
- **Multi-spectral reflectance imaging** → skin chromophore mapping for diagnostics, follow-up and self-monitoring
- **Autofluorescence intensity, lifetime and photobleaching rate imaging** → skin cancer diagnostics
- **Photoplethysmography imaging** → distant cardiovascular monitoring - e.g. heart rate and arrhythmia, anaesthesia control (Marta Lange, tomorrow)

SkImager: a proof-of-concept prototype

- Wireless, touch-screen, microcomputer
- Performs complex multimodal skin imaging by recording:
 - RGB reflectance image at white polarized illumination → revealing subcutaneous structures
 - 4 spectral images (450, 540, 660, 940nm) → distribution maps of melanin, haemoglobin, bilirubin, erythema index, melanoma/nevus index
 - Photoplethysmography video-image at green illumination → PPG amplitude distribution → skin blood perfusion map
 - Autofluorescence video-image at UV-excitation → map of photo-bleaching rates → skin fluorophore map

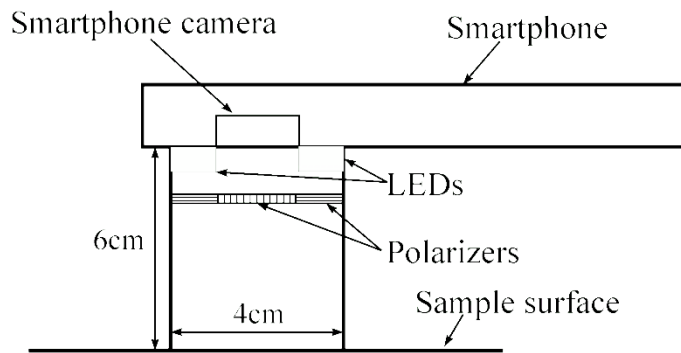


Inside

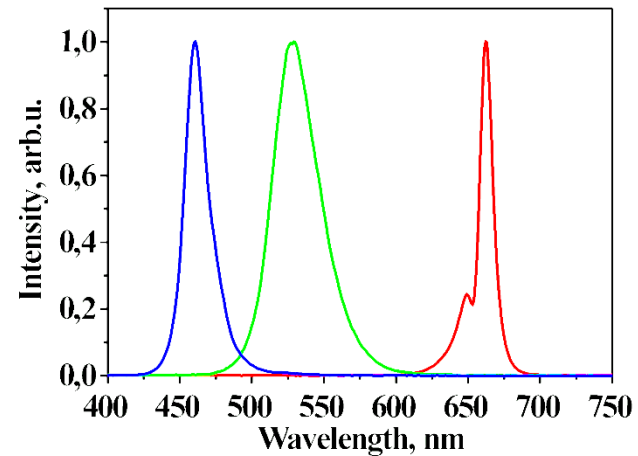


J.Spigulis, et al. Sklmager: a concept device for *in-vivo* skin assessment by multimodal imaging. *Proc.Est.Acad.Sci.*, 63(3), 213-220 (2014).

RGB-LED smartphone system for multispectral skin imaging



(a)

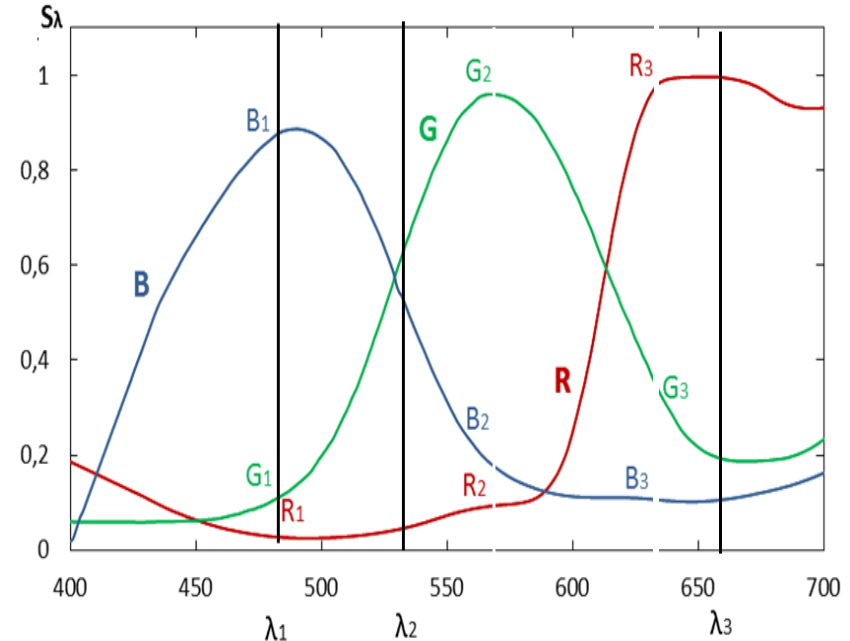
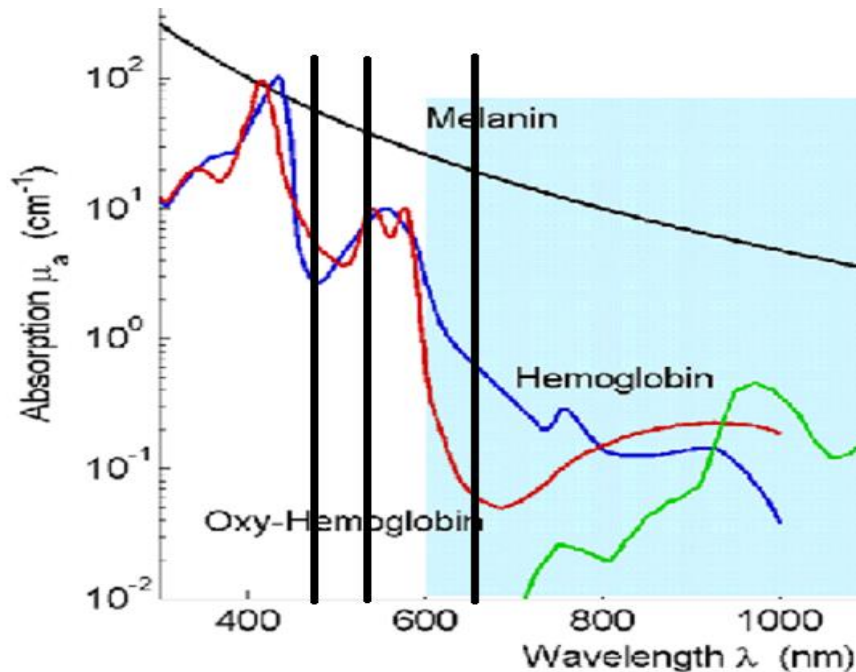


(b)

Kuzmina I., et al. Study of smartphone suitability for mapping of skin chromophores.
J.Biomed.Opt., **2015**, 20(9): 090503

Multi-monochromatic spectral imaging

- 3 **monochromatic spectral images** from a **single-snapshot RGB image** data can be extracted if object (skin) is illuminated simultaneously by 3 laser lines, and the RGB-band sensitivities of the image sensor are known
- Next step – conversion of 3 monochromatic spectral images into distribution maps of 3 main skin chromophores (Beer's-Lambert law \rightarrow 3 equations)

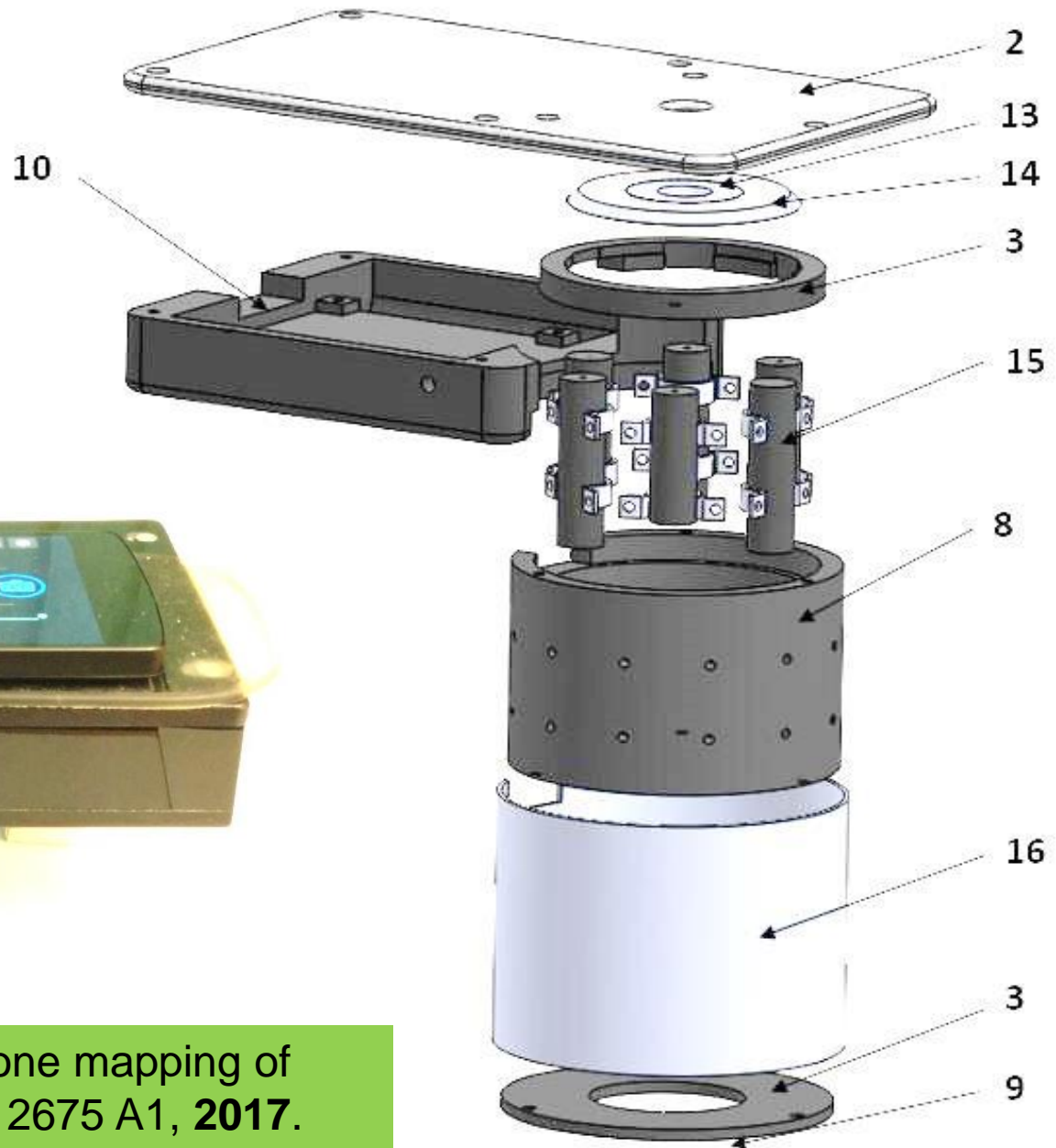


Method and device for imaging of spectral reflectance at several wavelength bands. WO 2013135311 (A1), 2012.

Smartphone add-on triple wavelength laser illuminator: 450nm, 532nm, 659nm

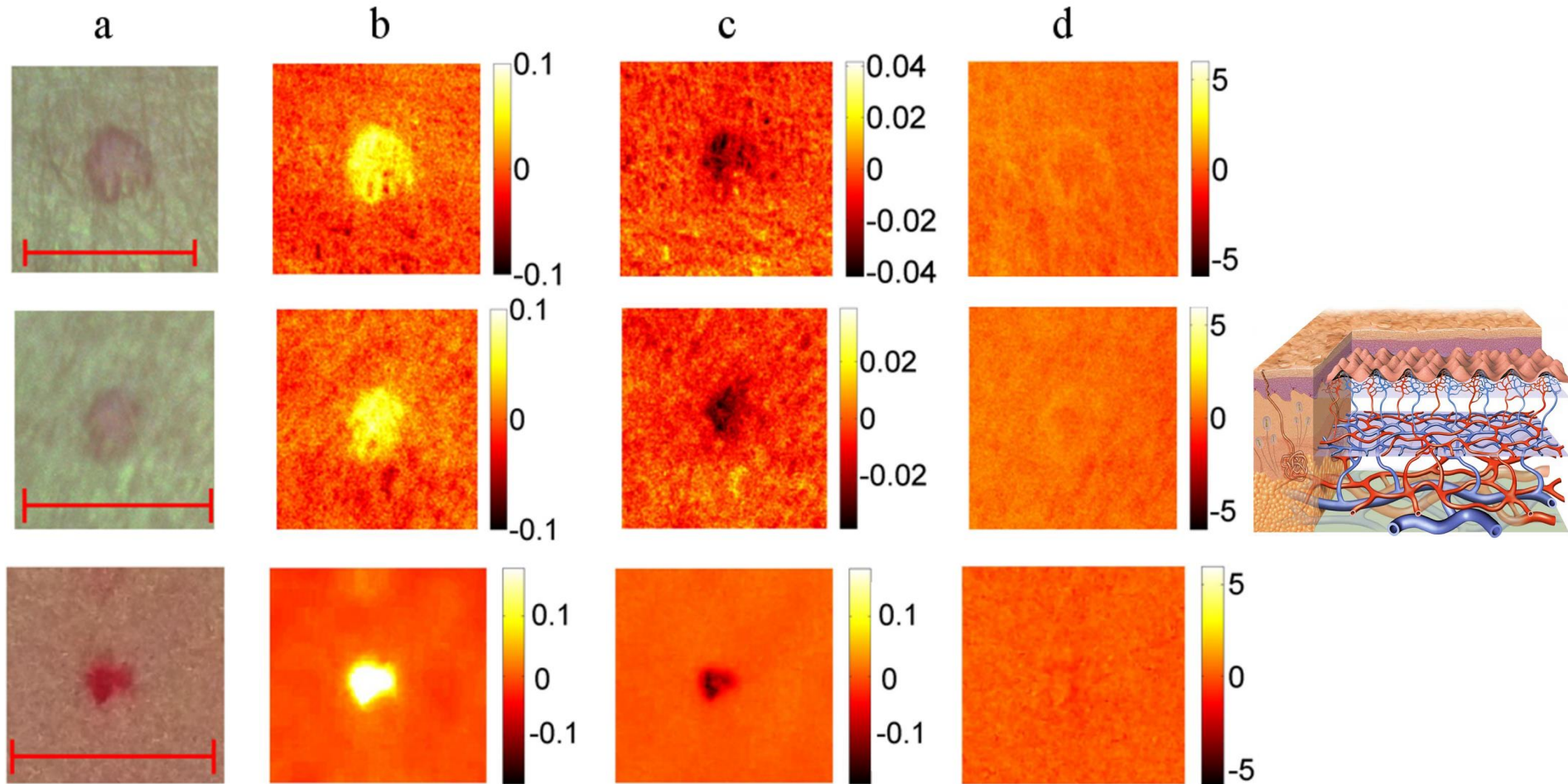


Method and device for smartphone mapping of
tissue compounds. WO 2017/012675 A1, **2017**.



RGB image (a) and maps of chromophore content changes for 3 vascular hemangiomas:

b – oxy-hemoglobin, c – deoxy-hemoglobin, d – melanin



Smartphone forensics:

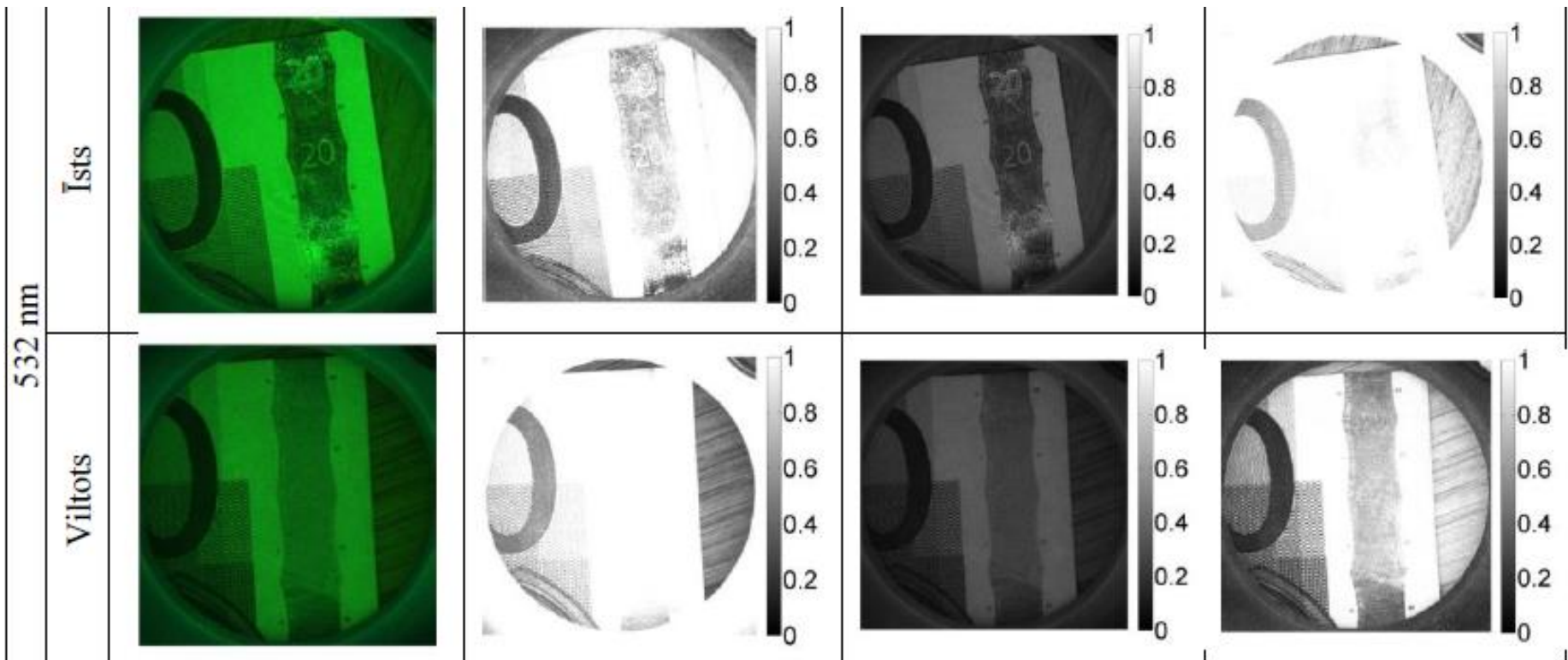
532nm monochromatic spectral images of authentic (upper row) and counterfeit (lower row, withdrawn by Bank of Latvia) 20 EUR banknotes

RGB

R

G

B

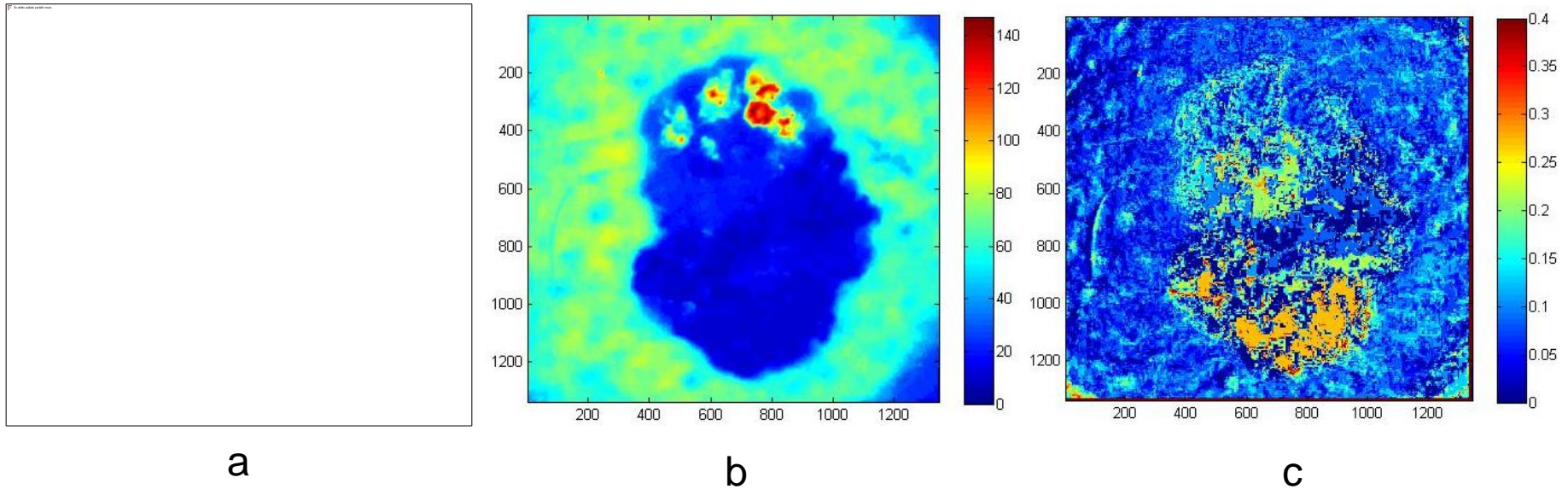


Smartphone fluorescent skin diagnostics



Atypical skin nevus

Smartphone RGB photo under 405nm LED irradiation



a

b

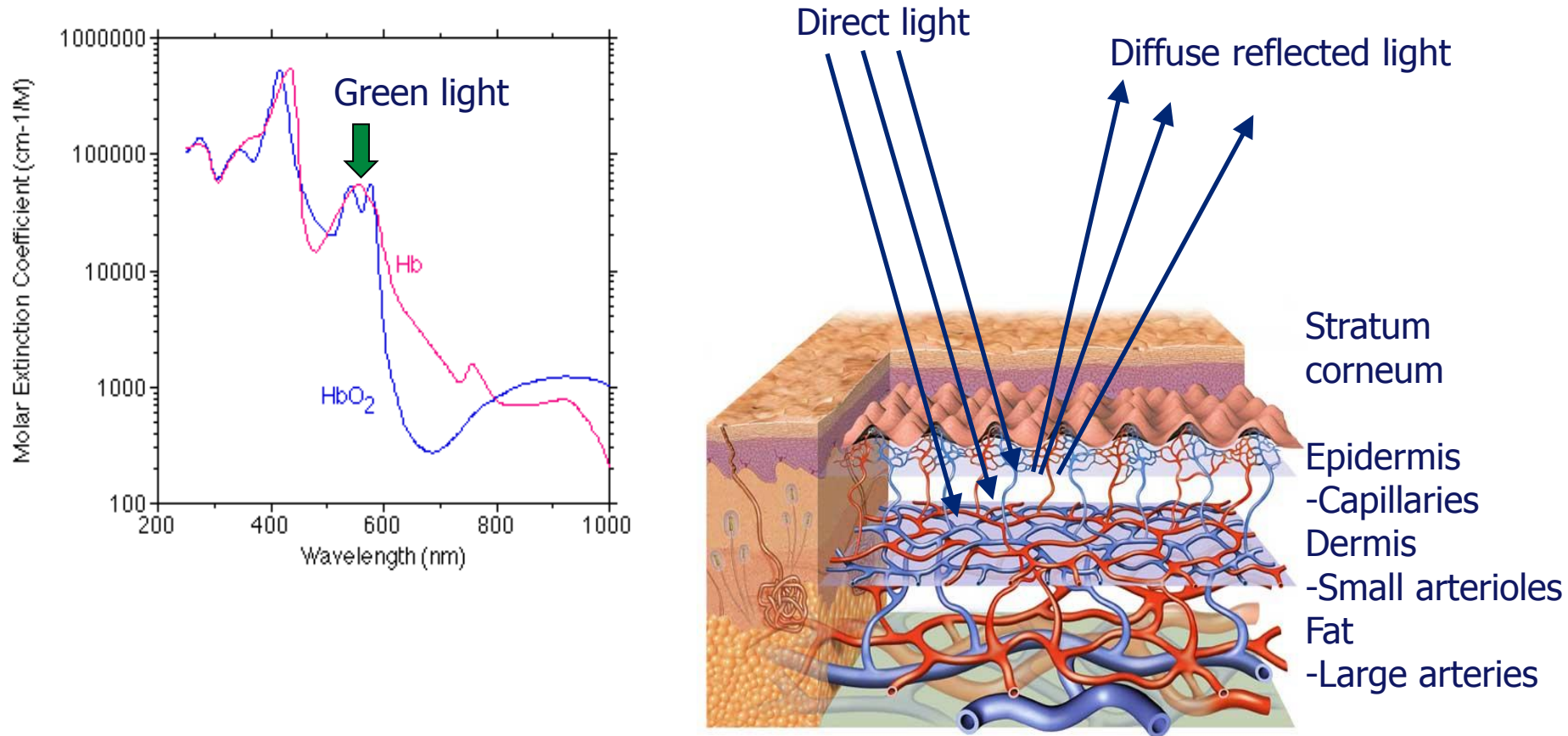
c

Filtered color image (a), AF intensity G-band image (b) and photobleaching rate map (c).

Histological analysis of the removed tissue samples confirmed three different types of tissue cells within the lesion area: the upper part mostly prevailed by intradermal nevus, the middle part by dysplastic nevus, and the lower part by junctional nevus.

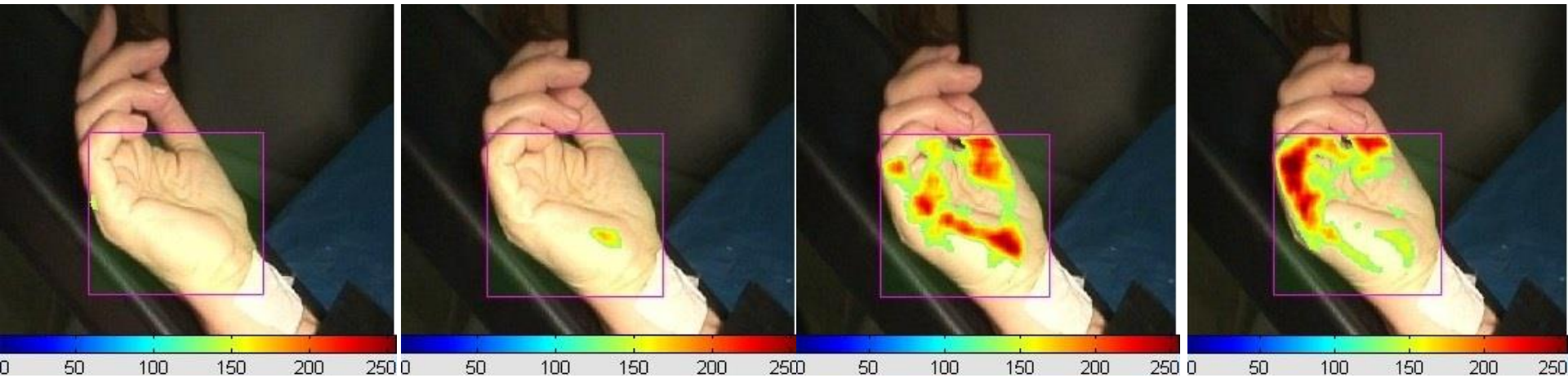
A.Lihachev, et al. Autofluorescence imaging of Basal Cell Carcinoma by smartphone RGB camera. *J.Biomed.Opt.*, 20(12), 120502 (2015).

Photoethysmography imaging: principle



PPGI: non-invasive technique for distant detection of blood flow pulsations in skin by analysis of backscattered optical radiation

PPGI for remote anaesthesia monitoring

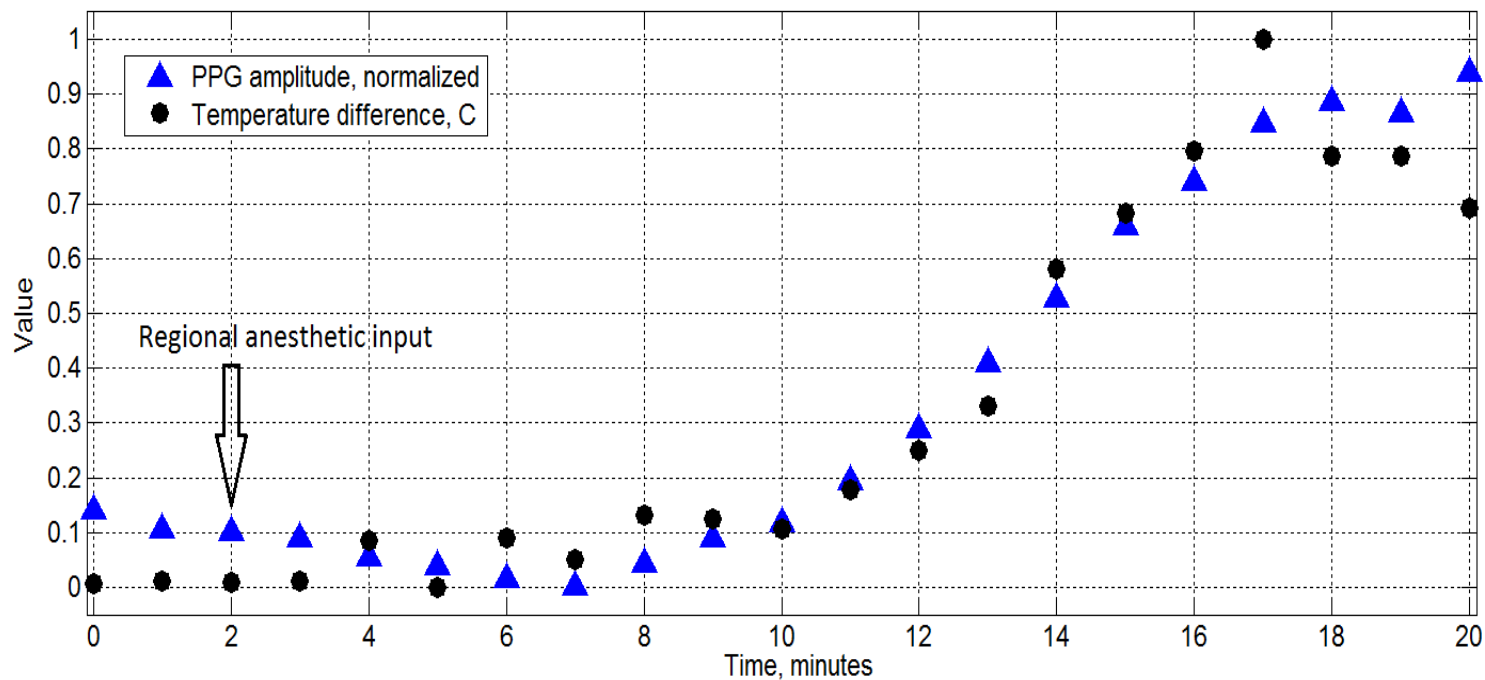


RA injection

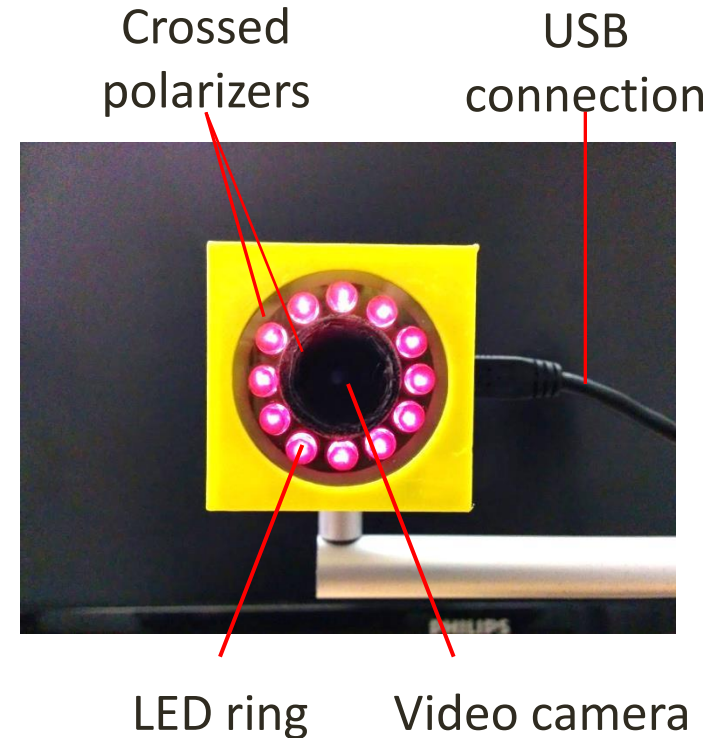
8 minutes

12 minutes

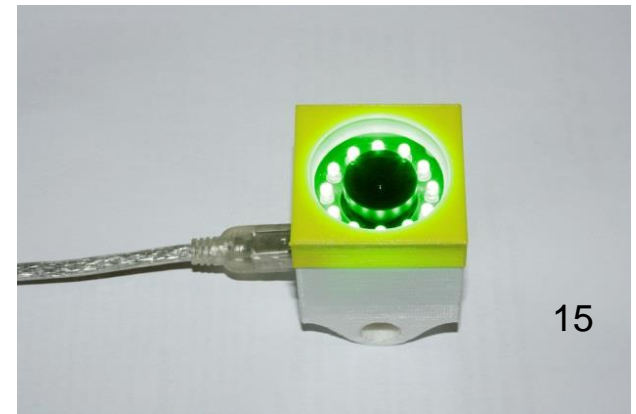
16 minutes



Compact (4x4x4 cm) prototype for remote blood perfusion mapping

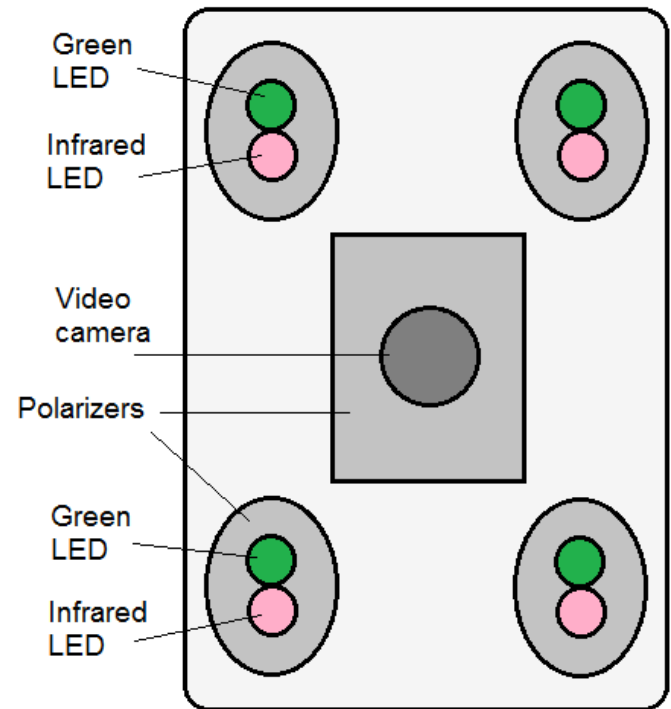


IR LED (760nm) – for measurements of deep layers of skin; green LED (540nm) – for measurements of upper layers of skin



Clinical prototype for remote anaesthesia control before/during palm surgeries

1. The device has vacuum pillow for fixing of palm in steady position.
2. Four bispectral illuminators perform uniform illumination of skin.



IR LED (810nm) – for measurements of deeper layers of skin; green LED (530nm) – for measurements of superficial layers of skin

Recent review paper: more details



Review

Multispectral, Fluorescent and Photoplethysmographic Imaging for Remote Skin Assessment

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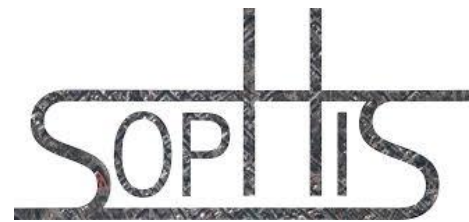
Sensors **2017**, *17*, 1165; (open access)

Summary

- Optical imaging techniques show promising potential for distant evaluation of *in-vivo* skin:
 - Multispectral imaging-based skin chromophore mapping
 - Fluorescence photobleaching-based skin fluorophore mapping
 - Remote photoplethysmography-based skin blood perfusion mapping
- Clinical applications: patient-friendly skin cancer screening, anaesthesiology control, burns, recovery monitoring, forensics, ...
- Research and commercial partners are welcomed!¹⁸

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Thank You!

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